

Beating heart simulation driven by three dimensional molecular dynamics model

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Heart + Cell + Motor proteins Multiscale Challenge on K-computer (2012)

FEM FEM MonteCarlo

Model size

macro	#myocardial elements	659456
micro	#myofibril elements of a cell	5796
	NDOF of a cell	49245
	NDOF of a z disk	230
	#motor proteins	160

Performance

model \ #nodes	Pflop/s			% of peak		
	20736	41472	82944	20736	41472	82944
49KDOF	0.72	1.39	2.74	28.10	27.43	27.72

II B Coronary Circulation

$$\sum_{c(x,t)=c} \bar{n}_x (\bar{\mu}_c - \bar{\mu}_{c(x,t)}) = 0, \forall c \quad (c)$$

$$\sum_{c(k,j)=c} \left(\frac{\pi}{4} D_{kj} \dot{D}_{kj} L_k + \eta_k (\mu_c - \mu_{c(k,j)}) \right) = 0, \forall c \quad (d)$$

$$D_i(t) = \beta \cdot ((\mu_i(t) - \bar{p}_m(t)) - (\mu_i^* - \bar{p}_m^*)) + D_i^* \quad (e)$$

$$\Delta V_{cap} = \bar{\omega} \frac{\pi}{8} \sum_k L_k \sum_{i=1}^2 (D_{ki}^2 - D_{ki}^{0,2}) \quad (f)$$

II A Macroscopic Muscle and Blood

$$\int_{\Omega_f} \{ \delta \bar{\mathbf{v}} \cdot \rho_f \mathbf{a}_f + 2 \mu_f \delta \bar{\mathbf{D}}_f : \bar{\mathbf{D}}_f - \bar{p}_f \nabla_x \cdot \delta \bar{\mathbf{v}} \} d\bar{\mathbf{x}} \quad \text{Blood}$$

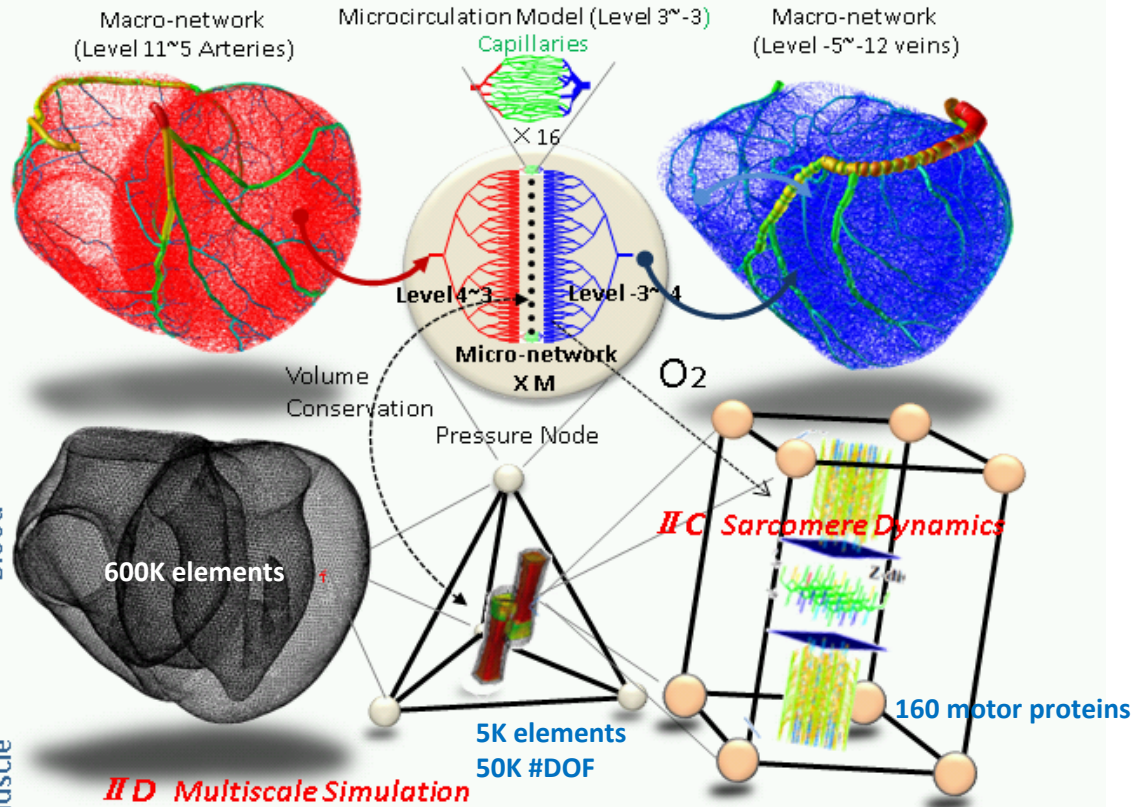
$$- \int_{\Gamma_f} \delta \bar{\mathbf{v}} \cdot \bar{\mathbf{v}}_f d\bar{s} + \int_{\Omega_f} \delta \bar{\mathbf{p}}_f \nabla_x \cdot \bar{\mathbf{v}} d\bar{\mathbf{x}}$$

$$+ \int_{\Omega_X} \delta \bar{\mathbf{u}} \cdot \bar{\rho}_s \ddot{\bar{\mathbf{u}}} d\bar{\mathbf{X}}$$

$$- \int_{\Omega_X} \delta \bar{J} \cdot \bar{p} d\bar{\mathbf{X}} + \int_{\Omega_X} \delta \bar{\mathbf{p}} \cdot (\bar{J} - 1 - \Delta V_{cap}) d\bar{\mathbf{X}} \quad *1$$

$$+ \int_{\Omega_X} \frac{1}{|\Omega_{\bar{\mathbf{X}}}|} \int_{\Omega_{\bar{\mathbf{X}}}} \delta \bar{\mathbf{W}} \cdot d\bar{\mathbf{X}} d\bar{\mathbf{X}} = 0 \quad (a)$$

$$\bar{J} = \det \bar{\mathbf{F}} = \det(\mathbf{I} + \partial \bar{\mathbf{u}} / \partial \bar{\mathbf{X}}) \quad (b)$$



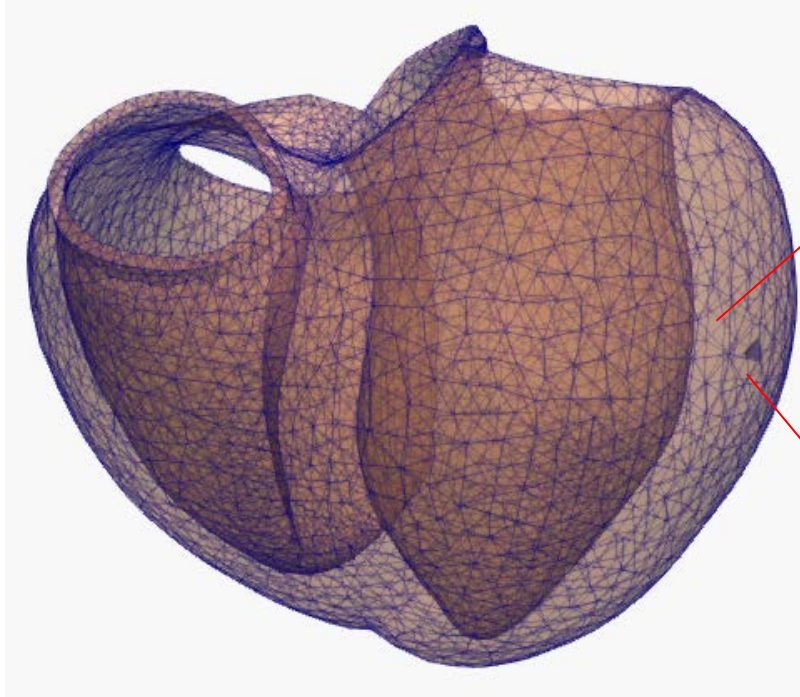
II D Multiscale Simulation

$$\bar{\mathbf{u}}(\bar{\mathbf{x}}) = \bar{\mathbf{R}}^T \bar{\mathbf{Z}} \bar{\mathbf{R}} \bar{\mathbf{x}} + \bar{\mathbf{w}}(\bar{\mathbf{x}}) \quad (g)$$

$$\bar{\mathbf{z}} = \frac{\partial \bar{\mathbf{u}}}{\partial \bar{\mathbf{x}}} \quad \bar{\mathbf{Z}} = \frac{\partial \bar{\mathbf{u}}}{\partial \bar{\mathbf{X}}} \quad \mathbf{u}(\mathbf{X}) = \mathbf{I}_{xy} \frac{1}{2} \bar{\mathbf{R}}^T (\bar{\mathbf{Z}} + \bar{\mathbf{Z}}^T) \bar{\mathbf{R}} \mathbf{X} + \mathbf{w}(\mathbf{X}) \quad (h)$$

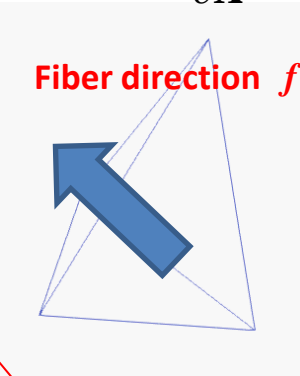
Conventional Multiscale Approach

Heart –Sarcomere Coupling Model



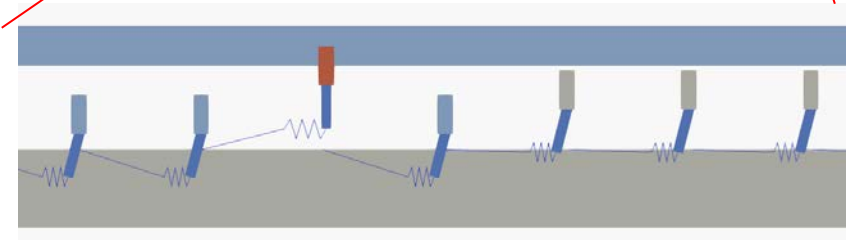
Strain tensor \mathbf{F} \rightarrow Length change in the fiber direction f \rightarrow Sarcomere length

$${}^t \mathbf{F} = \frac{\partial {}^t \mathbf{x}}{\partial \mathbf{X}}$$
$${}^t SL = SL_0 \left\| {}^t \mathbf{F} \mathbf{f} \right\|$$



Stress tensor $\mathbf{\Pi}_{act}$ \leftarrow Contraction force

$${}^t \mathbf{\Pi}_{act} = \frac{C T_s}{\left\| {}^t \mathbf{F} \mathbf{f} \right\|} \mathbf{f} \otimes \mathbf{f} \cdot {}^t \mathbf{F}^T$$
$${}^t T_s = \sum_{i=1}^n \delta_{A,i} k_M {}^t x_i$$

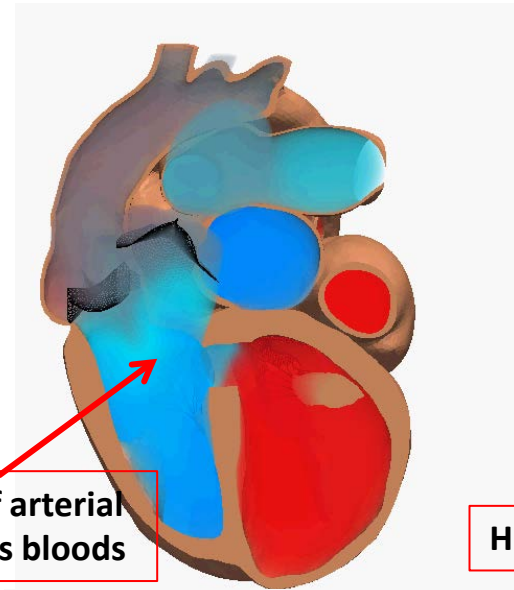


Filament sliding changes the mechanical load, thereby affects the lever arm swing and the detachment .

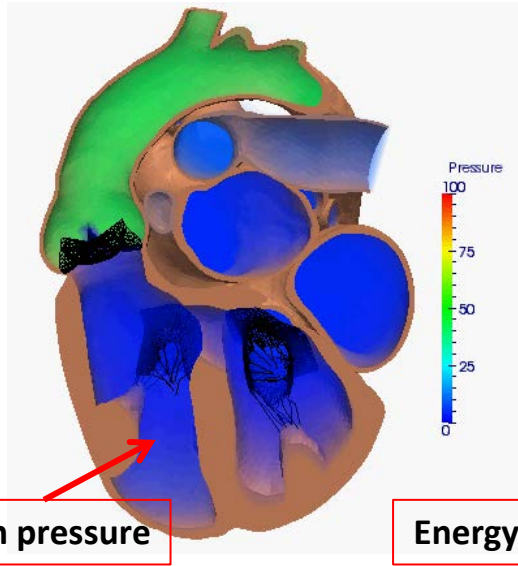
Application: Prediction of post-operation

Pre

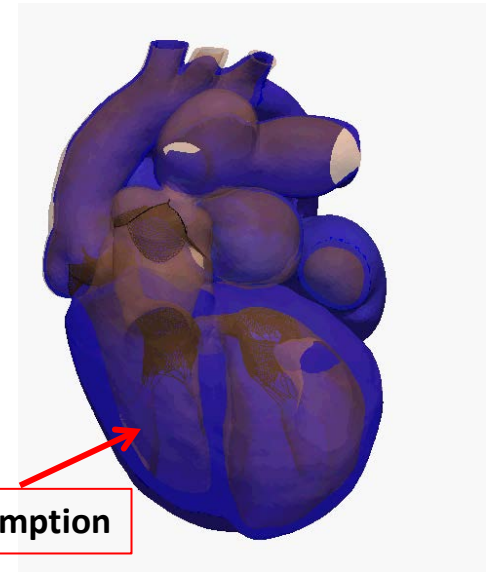
Mixture of arterial and venous bloods



High pressure

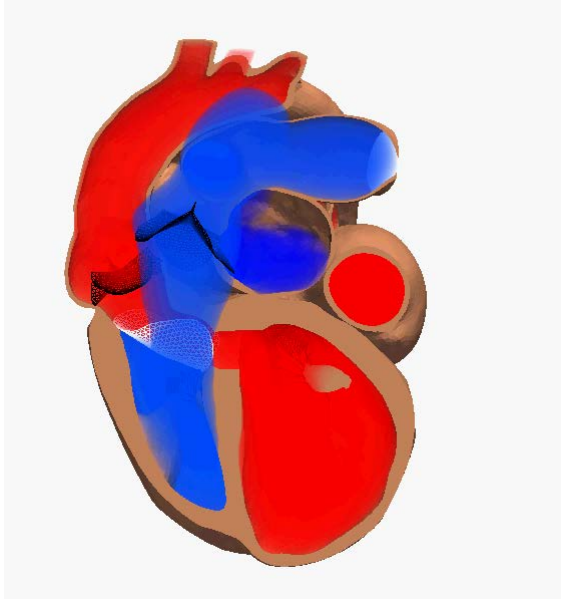


Energy consumption

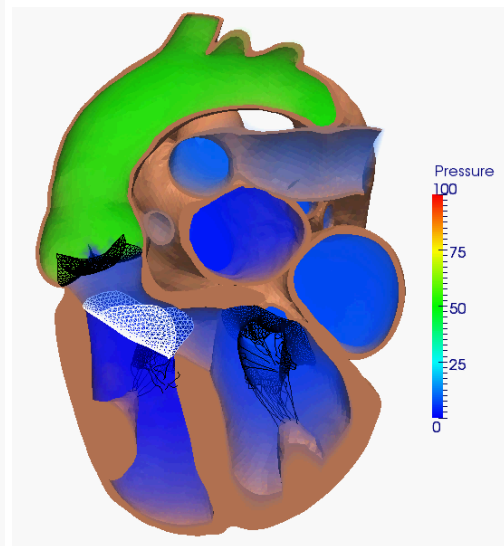


Post

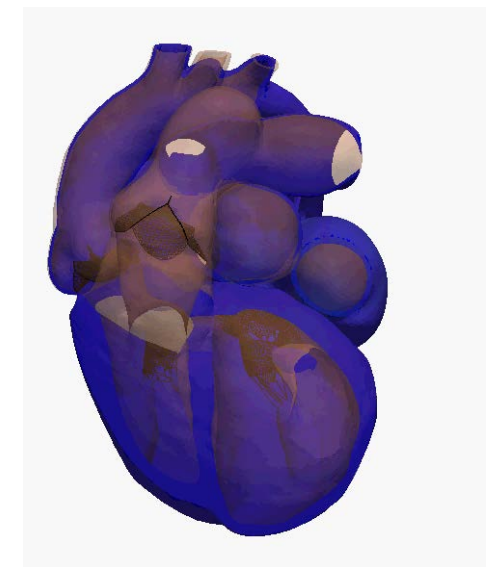
Improvement of SPO2



Load reduction
(RV blood pressure)



Energy saving
(RV energy consumption)



Research directions for Post-K : from 1d MC to 3d MD

K

1D Monte Carlo
Load dependent state Transition

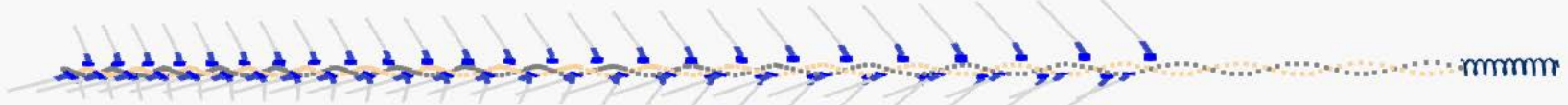
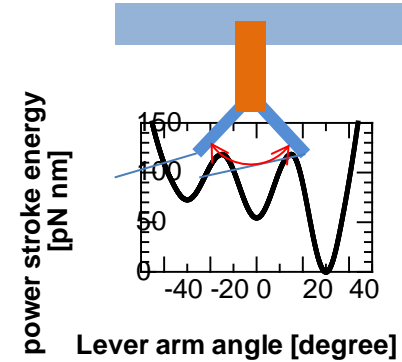
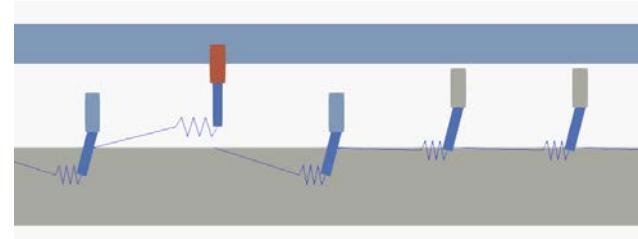


Post-K

3D Molecular Dynamics
Deformation potentials

Super Coarse grained (UT-Heart Inc.)

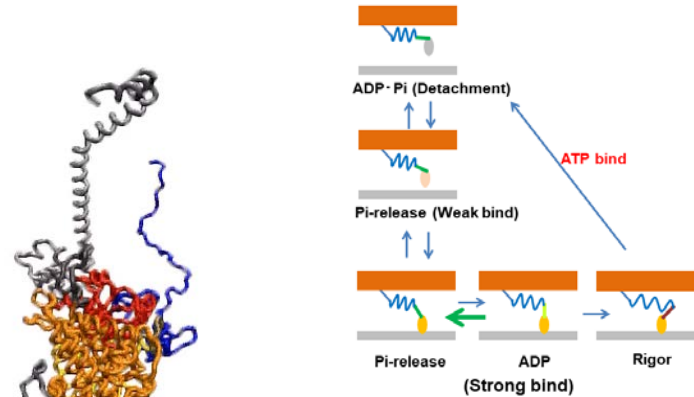
Focusing on 3D sarcomere structure



Cafemol (Takada Lab., Kyoto Univ.)

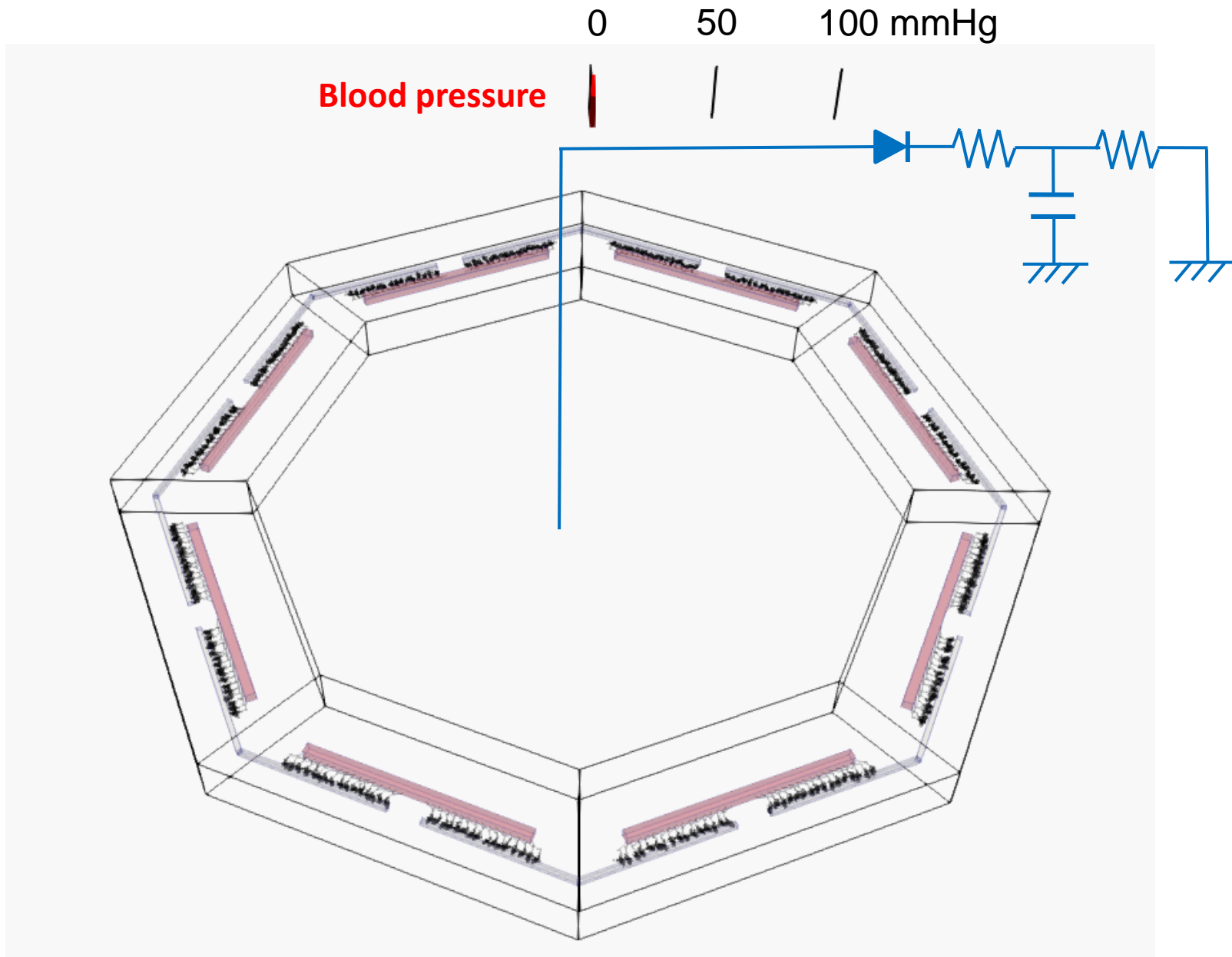
Focusing on inside of the molecular motor

Switch the potentials at the state transitions

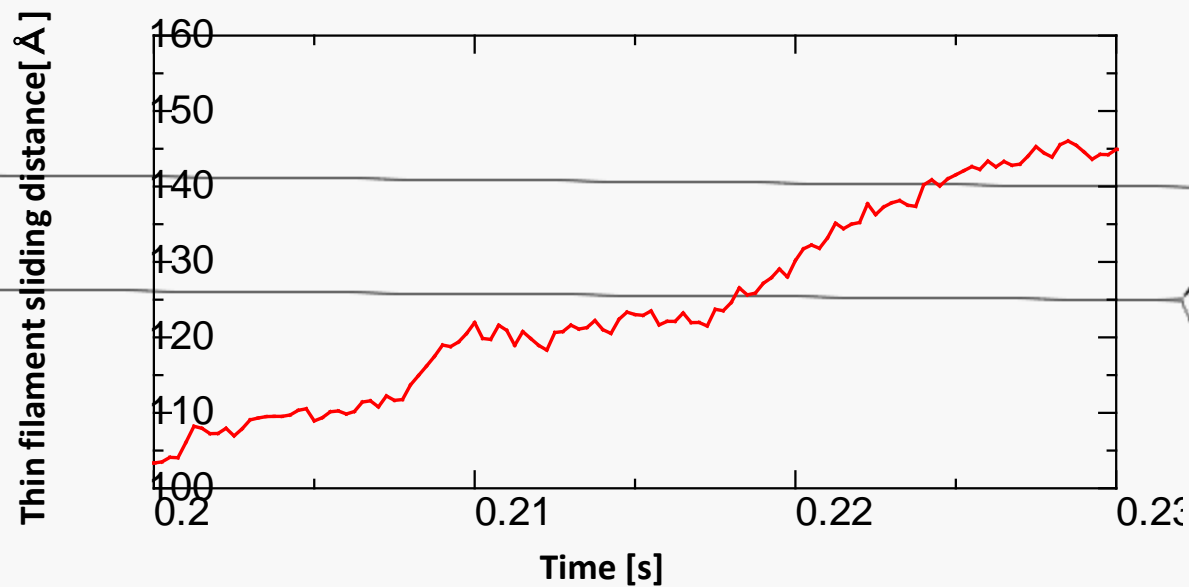


Thin filament (modeled by a rigid bar)

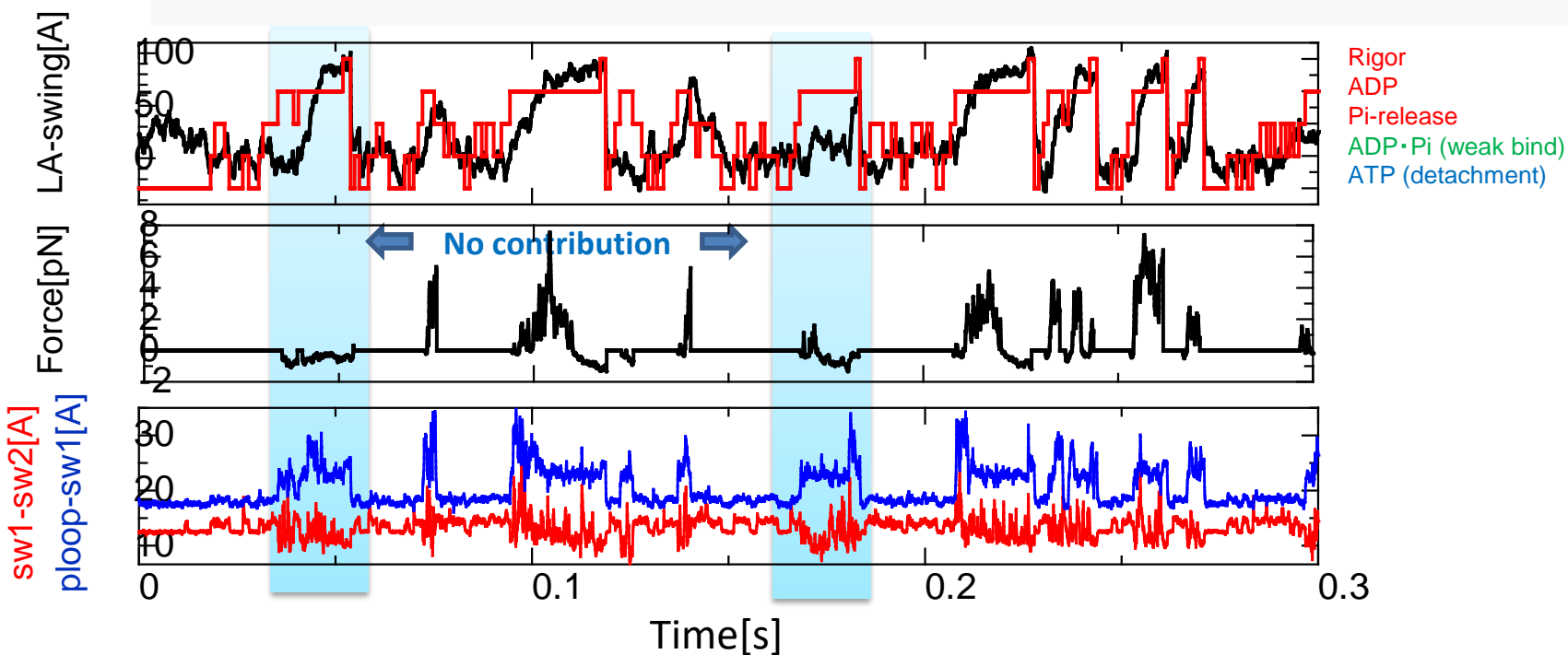
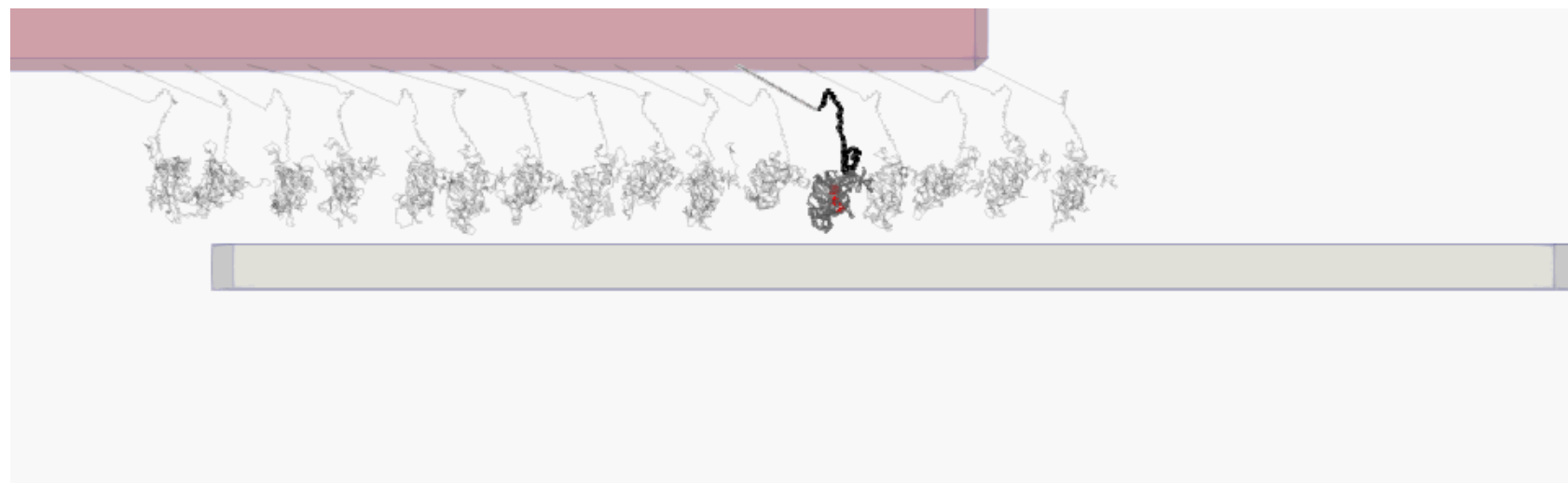
Preliminary test using Cafemol-Ring Coupling model



Micro-Macro interaction through the thin filament sliding



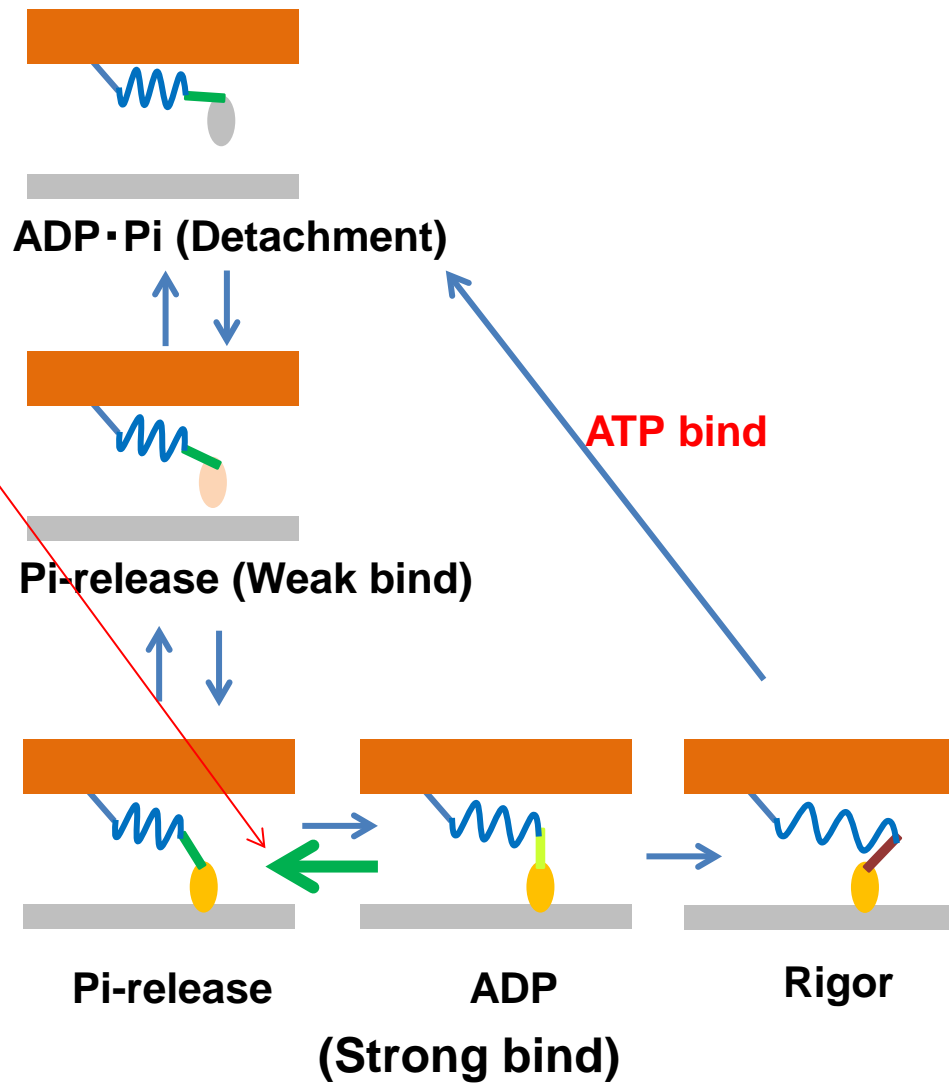
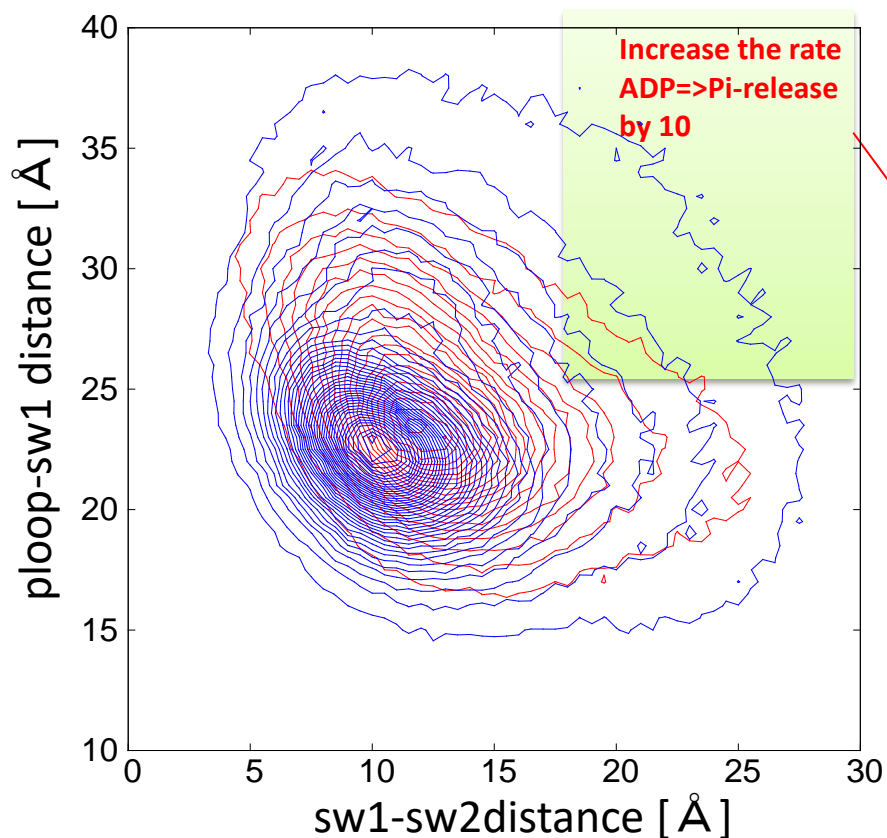
Behavior of the molecular motor under physiological condition



Verification of Pocket Deformation Feedback Model

Contour of the pocket deformation of the basic model

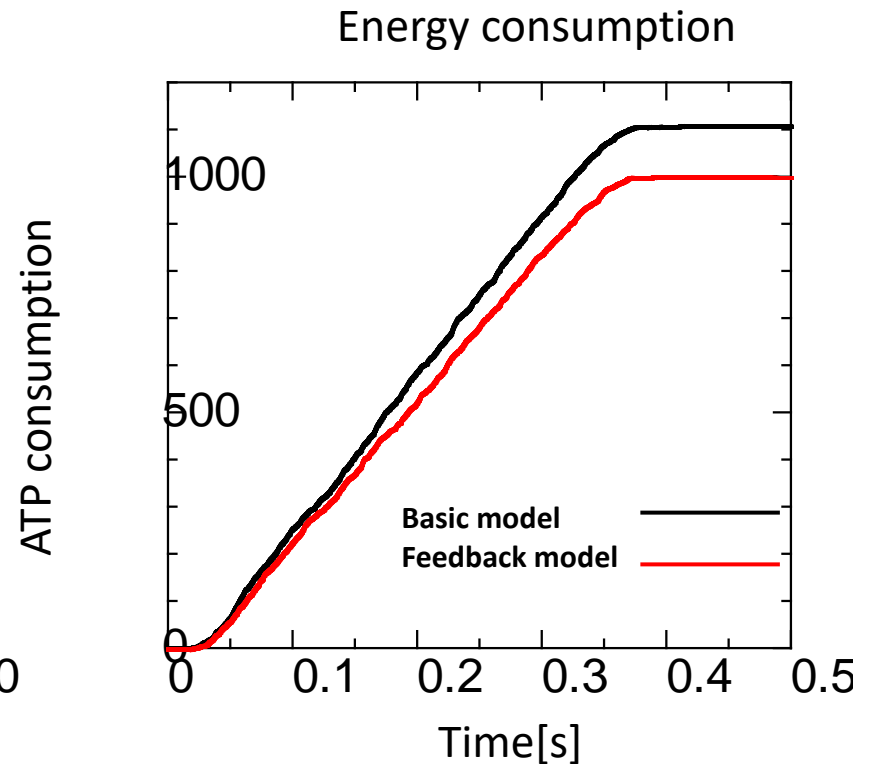
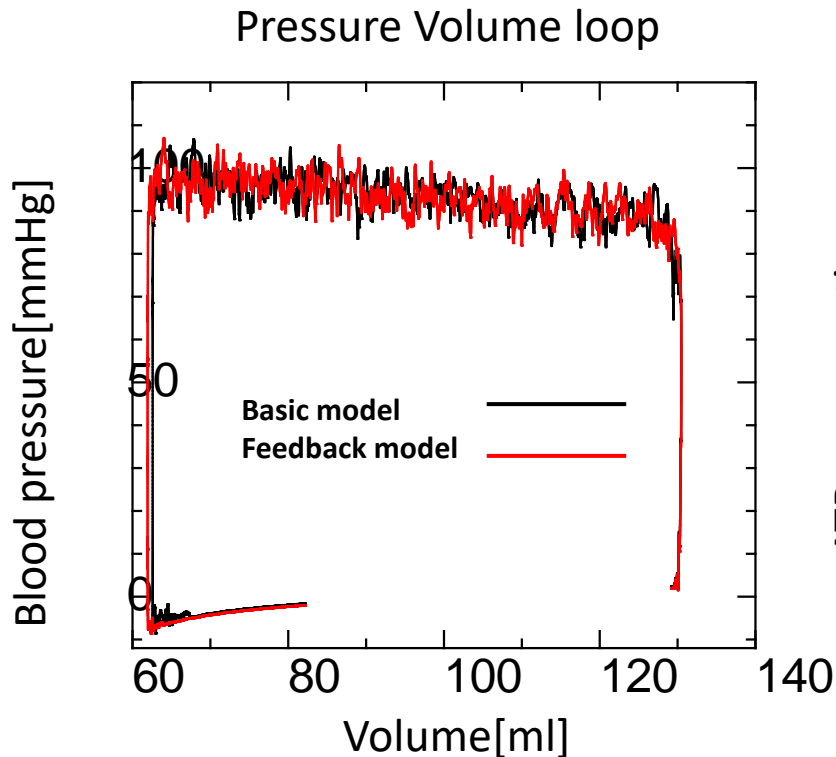
Red : successful cycles
Blue : unsuccessful cycles



Verification of Pocket Deformation Feedback Model

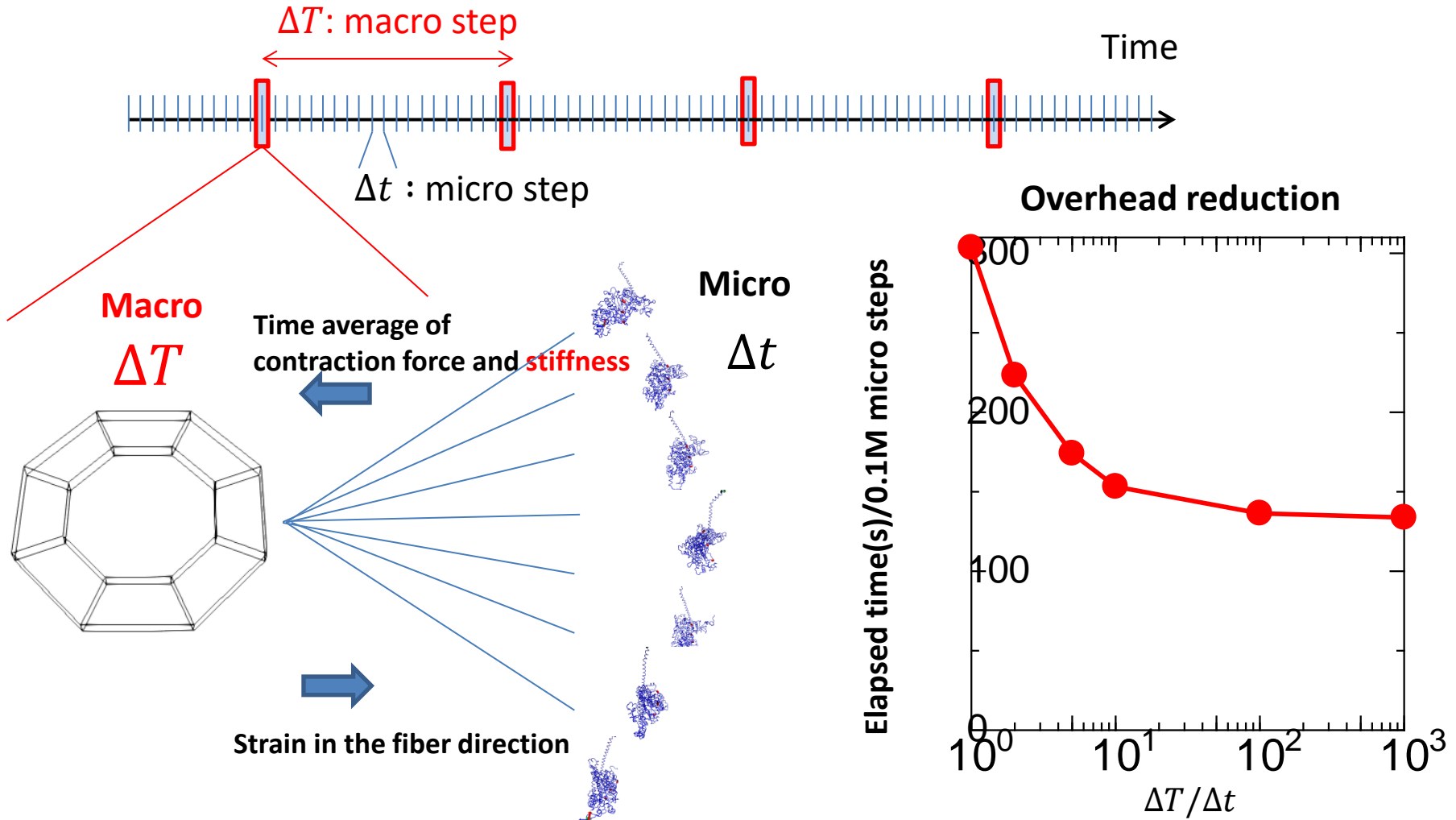
Benefits of the feedback mechanism

1. 3% increase of blood ejection
2. 10% reduction of ATP consumption



Coupling technique : Efficiency & Stability

1. Reduction of communication overheads by the multiple time step method
2. Stability by taking the active stiffness



Coupling technique : Efficiency & Stability

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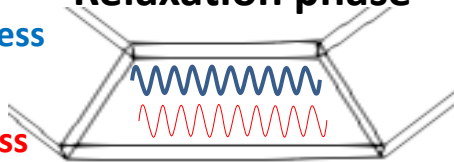
Macro

Relaxation phase

Passive stiffness

∇

Active stiffness

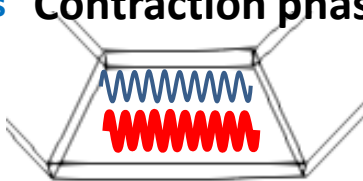


Passive stiffness

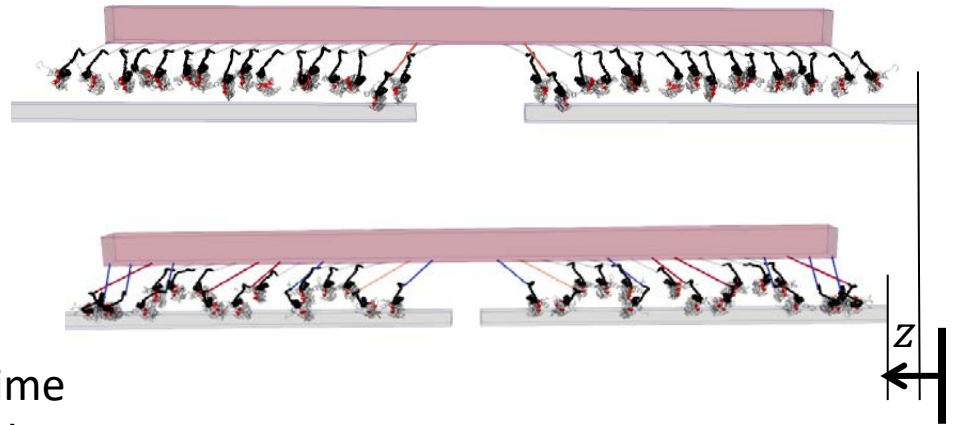
Contraction phase

∧

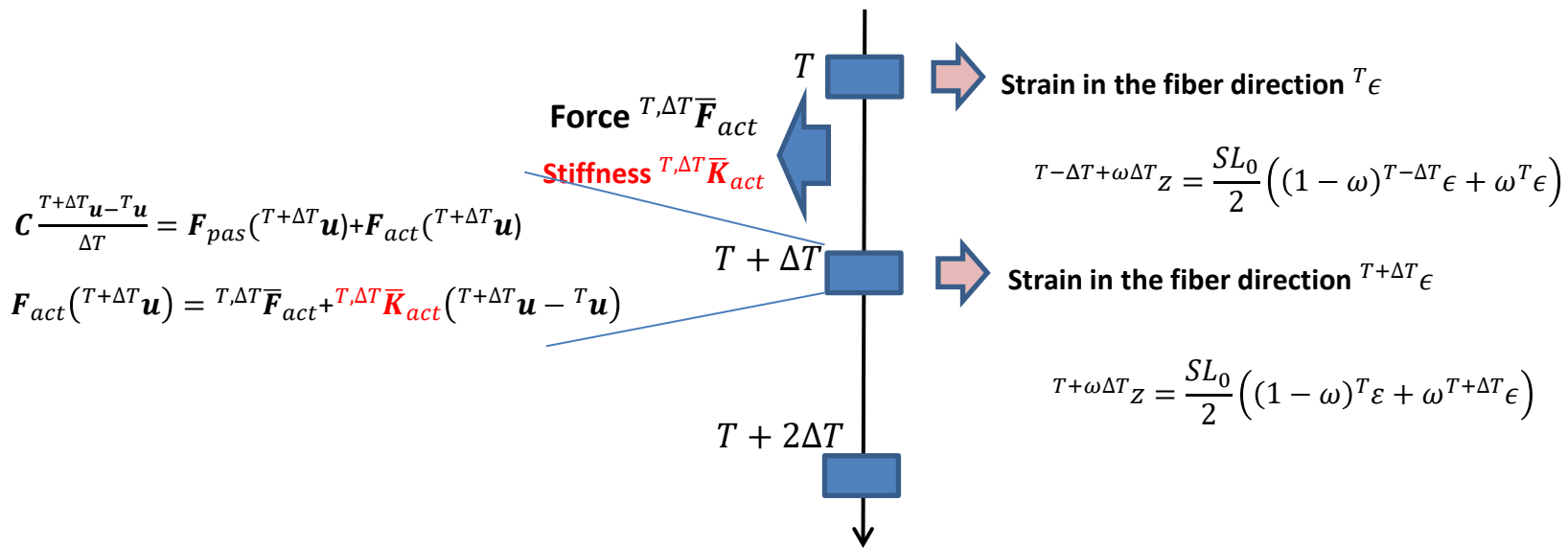
Active stiffness



Micro



Time

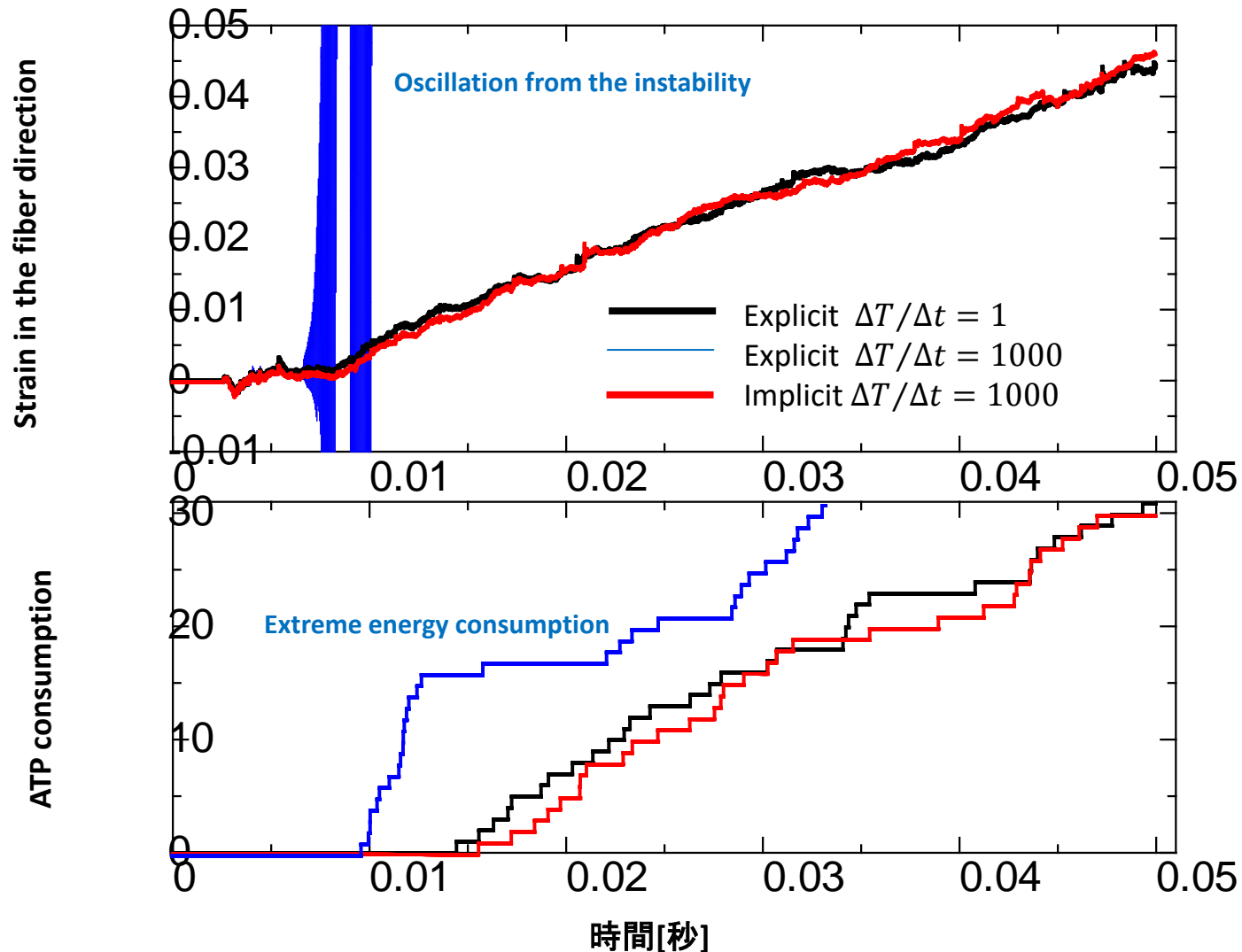


$$\mathbf{C} \frac{{}^{T+\Delta T}\mathbf{u} - {}^T\mathbf{u}}{\Delta T} = \mathbf{F}_{pas}({}^{T+\Delta T}\mathbf{u}) + \mathbf{F}_{act}({}^{T+\Delta T}\mathbf{u})$$

$$\mathbf{F}_{act}({}^{T+\Delta T}\mathbf{u}) = {}^{T,\Delta T}\bar{\mathbf{F}}_{act} + {}^{T,\Delta T}\bar{\mathbf{K}}_{act} ({}^{T+\Delta T}\mathbf{u} - {}^T\mathbf{u})$$

Coupling technique : Efficiency & Stability

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Concluding Remarks

We constructed a multiscale platform that enables us to analyze the stochastic dynamics of motor proteins under the condition :
that is **generated by the protein motors themselves**
that **can't be made from artificial boundary conditions**

Big data & AI

- Huge numerical simulation data of the molecular behavior
- Seeking correlations between the functional parts in the protein motors
- Optimization of parameters of numerical models

